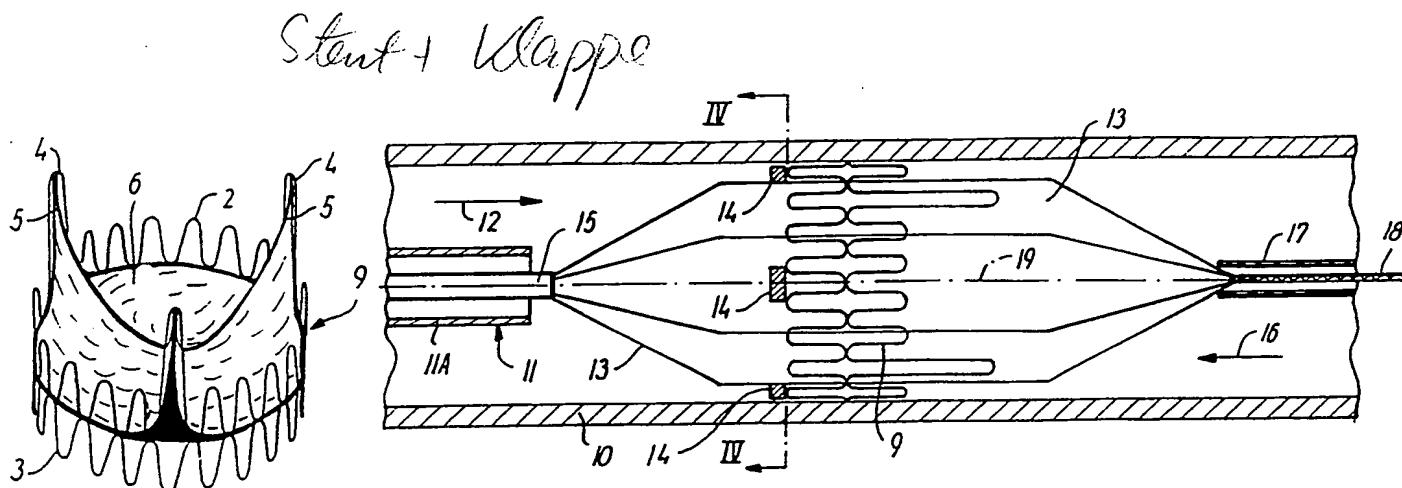


INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 5 : A61F 2/24, A61M 25/10		A1	(11) International Publication Number: WO 91/17720 (43) International Publication Date: 28 November 1991 (28.11.91)
(21) International Application Number: PCT/DK91/00134 (22) International Filing Date: 16 May 1991 (16.05.91)		(81) Designated States: AT (European patent), AU, BE (European patent), CA, CH (European patent), DE (European patent), DK (European patent), ES (European patent), FI, FR (European patent), GB (European patent), GR (European patent), IT (European patent), JP, LU (European patent), NL (European patent), NO, SE (European patent), US.	
(30) Priority data: 1246/90 18 May 1990 (18.05.90)		DK	
(71)(72) Applicants and Inventors: ANDERSEN, Henning, Rud [DK/DK]; Dalvangen 37A, DK-8270 Hoejbjerg (DK). HASENKAM, John, Michael [DK/DK]; Aprilvej 8, DK-8210 Aarhus V (DK). KNUDSEN, Lars, Lyhne [DK/DK]; Rudolf Wulffsgade 6, 4.mf, DK-8000 Aarhus C (DK).		Published <i>With international search report. In English translation (filed in Danish).</i>	
(74) Agent: LEHMANN & REE; Grundtvigsvej 37, DK-1864 Frederiksberg C (DK).			

(54) Title: A VALVE PROSTHESIS FOR IMPLANTATION IN THE BODY AND A CATHETER FOR IMPLANTATING SUCH VALVE PROSTHESIS



(57) Abstract

A valve prosthesis (9) for implantation in the body by use of catheter (11) comprises a stent made from an expandable cylinder-shaped thread structure (2, 3) comprising several spaced apices (4). The elastically collapsible valve (6) is mounted on the stent as the commissural points (5) of the valve (6) is secured to the projecting apices (4). The valve prosthesis (9) can be compressed around the balloon means (13) of the balloon catheter (11) and be inserted in a channel, for instance in the aorta (10). When the valve prosthesis is placed correctly the balloon means (13) is inflated thereby expanding the stent and wedging it against the wall of aorta. The balloon means is provided with beads (14) to ensure a steady fastening of the valve prosthesis on the balloon means during insertion and expansion. The valve prosthesis (9) and the balloon catheter (11) make it possible to insert a cardiac valve prosthesis without a surgical operation comprising opening the thoracic cavity.

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	ES	Spain	MG	Madagascar
AU	Australia	FI	Finland	ML	Mali
BB	Barbados	FR	France	MN	Mongolia
BE	Belgium	GA	Gabon	MR	Mauritania
BF	Burkina Faso	GB	United Kingdom	MW	Malawi
BG	Bulgaria	GN	Guinea	NL	Netherlands
BJ	Benin	GR	Greece	NO	Norway
BR	Brazil	HU	Hungary	PL	Poland
CA	Canada	IT	Italy	RO	Romania
CF	Central African Republic	JP	Japan	SD	Sudan
CG	Congo	KP	Democratic People's Republic of Korea	SE	Sweden
CH	Switzerland	KR	Republic of Korea	SN	Senegal
CI	Côte d'Ivoire	LI	Liechtenstein	SU	Soviet Union
CM	Cameroon	LK	Sri Lanka	TD	Chad
CS	Czechoslovakia	LU	Luxembourg	TC	Togo
DE	Germany	MC	Monaco	US	United States of America
DK	Denmark				

A VALVE PROSTHESIS FOR IMPLANTATION IN THE BODY AND A CATHETER FOR IMPLANTATING SUCH VALVE PROSTHESIS.

Background of the Invention.

5 The present invention relates to a valve prosthesis, preferably a cardiac valve prosthesis, for implantation in the body by means of a technique of catheterization and of the type comprising a collapsible elastical valve which is mounted on an elastical stent.

10 Valve prostheses of this type are usually implanted in one of the channels of the body to replace a natural valve. In the present description the invention will be explained in connection with an cardiac valve prosthesis for implantation in aorta. However, it will be possible to use a valve prosthesis according to the invention in connection with implantation in other channels in the body by using the 15 same technique as the one used for implantation of cardiac valve prosthesis. Such an implantation may e.g. comprise the implantation of:

1. a valve (for instance a cardiac valve) in the veins,
2. a valve in the oesophagus and at the stomach,
3. a valve in the ureter and/or the vesica,
20 4. a valve in the biliary passages,
5. a valve in the lymphatic system, and
6. a valve in the intestines.

25 An existing natural valve in the body is traditionally replaced with a valve prosthesis by a surgical implantation. However, a surgical implantation is often an exacting operation. Thus, today the implantation of cardiac valves are solely made by surgical technique where the thoracic cavity is opened. The operation calls for the use of a heart and lung machine for external circulation of the blood as the heart is 30 stopped and opened during the surgical intervention and the artificial cardiac valves are subsequently sewed in.

35 Due to its exacting character it is impossible to offer such operation to certain people. For instance this is due to the fact that the person is physically weak because of age or illness. Moreover, the number of heart and lung machines available at a hospital will be a substantially limiting factor.

Cardiac valve prostheses that need no surgical intervention are known

as there are used for implantation by means of a technique of catheterization. Examples of such valve prostheses are described in US Patent specifications Nos. 3,671,979 and 4,056,854. However, both these valve prostheses are connected to means which lead to the surface of the patient either for a subsequent activation of the valve or for a subsequent reposition or removal of the valve prosthesis. With these valve prostheses it is impossible to make an implantation which makes it possible for the patient to resume a substantially normal life in the same way as it is possible in connection with a surgical implantation of a cardiac valve.

From US Patent specification No. 3,755,823 an elastic stent for a cardiac valve prosthesis is known. However, this valve prosthesis is not designed for implantation in the body by catheterization. Even though the Patent specification contains no detailed explanation the description indicates that this valve prosthesis is designed for implantation and sewing on by a surgical intervention.

Moreover, from the US Patent specifications Nos. 4,856,516 and 4,733,665 different shapes of expandable stents are known. These stents are made to be expanded by impression of a radially outward force coming from a balloon catheter or the like. These stents are made to reinforce the wall when there is a risk that the channel is closed and/or compressed.

It is the object of the present invention to provide a valve prosthesis of the type mentioned in the introductory part, which permits implantation without surgical intervention in the body and by using a catheter technique known per se and which makes it possible for the patient to resume a substantially normal life.

This is achieved according to the invention with a valve prosthesis of the type mentioned in the introductory part, which is characterized in that the stent is made from an expandable cylindrical support means and that the commissural points of the elasical collapsible valve are mounted on the cylinder surface of the support means for folding and expanding together with the cylindrical support means.

The collapsible elastic valve is mounted on the stent for instance by

gluing, welding or by means of a number of suitable sutures.

If the support means are made from a thread structure this can for instance be grate shaped, loop shaped or helical. This makes it possible 5 to compress the stent and the collapsible valve mounted thereon for placing on the insertion catheter. The use of a non-self-expandable stent may e.g. be effected by a compression of the stent around the expansion arrangement of the catheter which preferably consists of a balloon. When using a self-expandable stent a catheter with an expansion 10 arrangement is not used. In this case the stent is compressed and is inserted into an insertion or protection cap from which the stent is eliminated after implantation in order to obtain an expansion due to the stresses in the compressed support means which for instance may be made from plastics or metal. After the compression the entire outer 15 dimension is relatively small which makes it possible to introduce the valve prosthesis through a channel in the body.

When the valve prosthesis is introduced and placed correctly the stent is expanded by self-expansion or by means of the expansion arrangement 20 until the stent is given an outer dimension which is slightly larger than the channel in which it is placed. As the stent is elastic a contraction of the stent is prevented once it is expanded. The stiffness in the material of the support means contributes to maintain the expanded shape of the stent. After the expansion is made the expansion 25 arrangement of the catheter is contracted and the catheter can be removed from the channel. The inlet opening can subsequently be closed and the patient will then be able to resume a normal life.

The valve prosthesis according to the invention does not require an 30 actual operation but merely a small intervention to optionally expose the body channel, e.g. a vein, through which the insertion takes place. Thus patients for whom operation will be associated with high risk can be offered implantation of for instance cardiac valves. After the implantation has taken place the after-treatment will advantageously 35 be shorter than normally which means fewer hospital days for the patient. Moreover, it is assumed that it will be possible to implantate the valve prosthesis under local anaesthetic.

The valve prosthesis can be used to replace a natural valve or to

establish a new valve function in one of the channels in the body which do not naturally contain a valve. For instance this goes for veins (arteries and veins) on a place without natural valves. The function of the valve prosthesis is then to ensure that the blood 5 flows in one direction only. The valve is meant to be used in veins in the legs of persons suffering from varicose veins (varices).

In persons having varicose veins the blood flows in a wrong direction, viz. from the central veins in the centre of the leg towards the 10 superficial veins. Among other things this is due to the changed pressure in the legs, upright working position and other conditions. A valve prosthesis according to the invention may easily be placed in the veins and prevent the flow of the blood in wrong direction.

15 Also, the valve prosthesis can be used in connection with diseases, for instance cancerous tumours, where too much humour is produced. If the humour is able to flow from the cancerous tumour through several channels it is possible to drain the humour in one desired direction through the channels of the body by an appropriate placing of the 20 valve prostheses.

When the valve prosthesis is used as cardiac valve prosthesis in the aorta it is possible to mount it in three positions, viz. in the descending part of the aorta, in a position between the coronary arteries 25 and the left ventricle of the heart or in the aorta in a position immediately after the mouth of the coronary arteries.

The cardiac valve prosthesis can also be used in other places than in the aorta. Thus the valve prosthesis can be used in the pulmonary artery and/or the right ventricle of the heart for replacing the pulmonary valves. Likewise the cardiac valve prosthesis can be used in the 30 passage between the right auricle of the heart and the right ventricle of the heart (tricuspidalostium) and the passage between the left auricle of the heart and the left ventricle of the heart (mistralostium) 35 for replacing the tricuspidal valve and the mitral valve, respectively.

Even though the cardiac valve preferably is meant to be used for patients suffering from aorta insufficiency and who can not be offered an open heart surgery the valve prosthesis can also be used for pa-

tients in connection with treatment of aorta stenosis. Several of the patients with aorta stenosis are elderly people who can not be offered a surgical cardiac operation. The patients are offered balloon dilatation of the aorta stenosis which may result in an aorta insufficiency as a side effect of the treatment.

As to these patients it is possible to insert a valve prosthesis in the descending or ascending part of the aorta thoracalis a few days or weeks before the balloon dilatation. As a result thereof the left ventricle is protected against weight if the subsequent balloon dilatation of the stenosis results in aorta insufficiency. In certain cases the weight (reflux) on the left ventricle is reduced by up to approximately 75%.

Furthermore, the stent may be made with a relatively great height and with a cylinder surface which is closed by a suitable material. Thus, a vascular prosthesis known per se is formed wherein the valve is mounted. This may facilitate the implantation of the valve prosthesis, for instance in the arcus aorta. Moreover, the great surface which abuts the inner wall of the channel contributes to ensure the securing of the valve prosthesis in the channel. This embodiment is also suitable as valve prosthesis which is inserted in veins. As veins have relatively thin and weaker walls than arteries it is desirable that the valve prosthesis has a greater surface to distribute the outward pressure which is necessary to secure the valve prosthesis.

Moreover, the invention relates to a balloon catheter for implantating a valve prosthesis according to the invention and comprising a channel for injection of a fluid for the inflation of the balloon means of the catheter and an insertion cap wherein the balloon means of the catheter and a collapsible valve prosthesis mounted thereon are located during the injection, characterized in that the balloon means are provided with a profiled surface which is made to ensure a steady fastening of the valve prosthesis during the elimination of the balloon means from the protection cap and the subsequent inflation for the expansion of the stent.

Different balloon catheters for implantating cores in the body are known. For instance such balloon catheters are known from US Patent

specifications Nos. 4,856,516, 4,733,665 and 4,796,629 and from DE publication No. 2,246,526. However, the known balloon catheters have a smooth or a slightly wavy surface. The use of such balloon catheter is disadvantageous for mounting a valve prosthesis in a channel having a 5 large flow as for instance the aorta. A large humour flow is able to displace the stent on the smooth surface of the balloon and makes an accurate positioning difficult. This drawback has been remedied with the balloon catheter according to the present invention as the profiled surface prevent a displacement of the valve prosthesis in relation 10 to the balloon means during introduction and the subsequent inflation of the balloon means.

In connection with the implantation any prior art technique may be used to supervise an accurate introduction and positioning of the valve 15 prosthesis. Thus, guide wires for the catheter, X-ray supervision, injection of X-ray tracable liquids, ultrasonic measuring etc. may be used.

Description of the Drawings.

20

The invention will now be explained in details with reference to the accompanying schematical drawing, wherein

25 Fig. 1 shows a perspective view of a stent without a valve,
Fig. 2 a perspective view of a valve prosthesis according to the invention made from the stent shown in Fig. 1 having a biological valve mounted thereon,
Fig. 3 a partiel view through the aorta illustrating a partially inflated balloon catheter,
30 Fig. 4 a cross section through the embodiment shown in Fig. 9,
Fig. 5-7 views illustrating the introduction and implantation of a valve prosthesis of the invention in the aorta,
Fig. 8-10 views illustrating three possible positions of a cardiac valve prosthesis, and
35 Fig. 11-12 perspective views illustrating two further embodiments of a valve prosthesis having a closed cylindrical wall.

Fig. 1 shows a stent 1 made by support means in the form of two 0,55 mm surgical stainless steel wires 2,3. The wires are folded in 15

loops. Three loops 4 are 14 mm in height and intended to secure the commissural points 5 (see Fig. 2) from a biological cardiac valve 6 which is mounted in the stent 1. The remaining loops have a height of 8 mm. Each of the two folded wires 2,3 was bended to form rings 7,8 which were closed by welding the ends. The two rings are place on the top of each other as will appear from Fig. 1 and they are mutually secured by means of a number of sutures (not shown). By using a substantially cylindrical thread structure with projecting apices a reduction in weight is obtained compared to a stent which is exclusively cylindrical with the same loop heights for all the loops.

The biological valve 6 was removed from a slaughtered pig of 100 kg. The valve was cleaned before mounting in the stent 1. The cleaned valve has an outer diameter of 25-27 mm and the height of the three commissural points 5 is 8 mm. The valve 6 is mounted in the stent by means of a suitable number of sutures to form the cardiac valve prosthesis 9 shown in Fig. 2. The valve prosthesis produced is used for performing tests in pigs by implantation of cardiac valve prosthesis. However, the cardiac valve prosthesis for use in human beings has a corresponding form.

Fig. 3 shows a partiel view through the aorta 10. A balloon catheter 11 is introduced in the aorta according to the direction of an arrow 12. In the Figure shown the balloon means 13 of the balloon catheter is led out of the protection cap 11A and is partly inflated through a fluid channel 15, which is led to the surface of the patient. The balloon means 13 constitutes a tri-sectional balloon upon which the cardiac valve prosthesis is placed. In the form shown the cardiac valve prosthesis is expanded exactly to be in contact with the aorta 10. The balloon means 13 is provided with three projecting beads 14 which are engaged with the one side of the cardiac valve prosthesis 9. The blood flowing through the aorta according to the direction of an arrow 16 will thus cause the cardiac valve prosthesis 9 to abut on the beads 14 and the valve cannot be displaced in relation to the balloon means 13. Moreover, the balloon catheter used comprises a central channel 17 to receive a guide wire 18 which is used in a way known per se for supervising the introduction of the catheter through fluoroscopi. In the shown embodiment beads 14 are only used at one side of the valve prosthesis, but, however, it will often be desirable to use the beads in

5 pairs placed along lines parallel to the longitudinal axes 19 through the balloon means 13. In this case the spacing of the pair of beads 14 will correspond to the height of the loops of the stent. This makes it provided by using balloon means with an indentation in the surface (not shown).

10 Fig. 4 shows a cross section through the embodiment shown in Fig. 3 illustrating the placing of the beads 14 on the tri-sectional balloon means 13.

15 A balloon catheter of the above described type which was used in tests of implantating the cardiac valve prosthesis 9 in pigs had the following dimensions. Each of the three balloons is 60 mm in length and 15 mm in diameter. The total diameter for the three inflated balloons is 31 mm and in the balloon catheter used two beads 14 having a height of 3 mm are mounted on each side of the three balloons. The beads have a spacing of 15 mm. The protection cap 11A of the balloon catheter has 20 an outer diameter of 13.6 mm and an inner diameter of 12.5 mm and a length of 75 cm. The balloon catheter is provided with a standard guide wire having a diameter of 0.9 mm and a length of 300 cm.

25 Figs. 5-7 show the valve prosthesis 9 at different steps in introducing and implantating in the aorta 10 by means of the catheter 11 having the inflatable balloon means 13. The cardiac valve prosthesis 9 is initially placed above the deflated balloon means 13 and compressed manually around the balloon means (Fig. 5), whereafter the outer diameter for the valve prosthesis is approximately 10 mm. After the introduction and positioning the balloon means 13 is inflated (Fig. 6) thereby contributing an outer dimension of approximately 30 mm to the cardiac valve prosthesis. To obtain an effective fastening in the aorta the outer dimension of the cardiac valve prosthesis is greater than the diameter of the aorta. This means that the prosthesis is tight 30 against the inner wall of the aorta with a pressure which is sufficiently large to counteract a detachment due to the flow of the blood. The balloon catheter 11 may subsequently be removed from the aorta 10 (Fig. 7). Due to the stiffness of the metal the valve prosthesis will 35 prevent a contraction. However, smaller contractions may occur (<10%

diameter reduction) after the deflation and removal of the balloon catheter 13. When the valve prosthesis is mounted as showed in Fig. 7 the patient will be able to resume a substantially normal life after a few days.

5

Figs. 8-10 show the positioning of the valve prosthesis 9 as cardiac valve prosthesis in the aorta 10 in three different positions. In a position between the coronary arteries 20 and the left ventricle of the heart 21 (Fig. 8). In a position immediately after the mouth of the coronary arteries in the ascending part of the aorta (Fig. 9). In a position in the descending part of the aorta 10. The positioning of the valve prosthesis is chosen in accordance with the diagnose of the illness of the patient. By placing the cardiac valve prosthesis as shown in Fig. 8 there is a risk of detachment and/or covering the mouth of the coronary arteries, and therefore it is preferred to use a higher stent which for instance comprises several rings 7,8 placed on top of each other. This allows a fixation of the prosthesis at a place after the mouth of coronary arteries even though the valve itself is in the position between the coronary arteries and the left ventricle. Fig. 8 and 9 show how a contrast medium 23 is injected by means of a so-called pigtail catheter for registration of the tightness of the implanted valve prosthesis 9.

25

A specific embodiment for a valve prosthesis and a balloon catheter for implantating the valve prosthesis has been explained above. However, it is obvious that it is possible to modify the valve prosthesis depending on the desired use, and moreover, it is possible to modify the catheter used in the implantation. Thus the stent of the valve prosthesis may be made solely of one closed ring folded in a number of loops or with three or more mutually secured loop-shaped rings placed on top of each other. Moreover, it is possible to make the stent having a thread structure which in stead of loops is grate shaped, helical or is formed otherwise if only it is ensured that the form of the stent permits the compression and expansion of the stent and fastening of the collapsible valve. In stead of a biological valve it might be possible to use other collapsible valves, such as valves made from synthetic materials, e.g. polyurethane. It is also possible to use valves with more or fewer flaps than three.

It is possible to make the valve prosthesis with a closed cylinder surface as illustrated in Figs. 11 and 12. In both Figures the support means of the valve prosthesis is made of an elongated tubular means 24 having a closed cylinder surface. This valve prosthesis is intended to 5 expand by self-expansion or by means of a catheter according to the invention. This prosthesis is especially suitable for placing in veins and other channels where only a small pressure is exerted against the wall of the channel. In Fig. 11 the valve 6 is mounted at the end of the tubular means 24. In Fig. 12 an embodiment is showed where the 10 valve 6 is mounted in a central position in the tubular means 24.

An explanation of a method of implantating a valve prosthesis according to the invention is given below:

15 - a valve prosthesis 9 made of a stent 1 and a collapsible valve 6, as described above,

- the valve prosthesis 9 is placed on a deflated balloon means and is manually compressed thereon,

- the balloon means 13 and the valve prosthesis are drawn into an insertion cover 11A,

20 - a guide wire 18 is inserted into the left ventricle of the heart through the central opening 17 of the balloon catheter under continuous fluoroscopi,

- the insertion cover 18 conveys the guide wire 18 to a point in the channel in immediate vicinity of the desired position of the valve prosthesis,

25 - the balloon means 13 is pushed out of the protection cap 11A and the valve prosthesis is positioned in the desired position if necessary by use of further registration means to ensure an accurate positioning,

30 - the balloon means 13 is inflated with a certain overstretching of the channel,

- the balloon means 13 is deflated, and

- the balloon means 13, the guide wire 18 and the protection cap 11A are drawn out and the opening in the channel, if any, wherein the valve prosthesis is inserted can be closed.

35

C L A I M S.

1. A valve prosthesis, preferably a cardiac valve prosthesis, for implantation in the body by means of a technique of catheterization and of the type comprising a collapsible elastical valve which is mounted on an elastical stent, characterized in that the stent is made from an expandable cylindrical support means and that the commissural points of the elastical collapsible valve are mounted on the cylinder surface of the support means for folding and expanding together with the cylindrical support means.
2. A valve prosthesis according to claim 1, characterized in that the support means is made of a thread structure.
- 15 3. A valve prosthesis according to claim 2, characterized in that the thread structure comprises several spaced apices projecting from the one side of the cylindrical structure and in direction along the longitudinal axis of the cylinder and that the commissural points of the valve are attached to the projecting apices.
- 20 4. A valve prosthesis according to claim 3, characterized in that the elastically collapsible valve is a biological trilobate valve.
- 25 5. A valve prosthesis according to claim 4, characterized in that the stent is made from a stainless steel wire folded in a number of loops and bended according to a circle and welded to form a closed ring, that the stent comprises two or more such closed rings which are mutually connected end to end to form the cylindrical thread structure, that three of the loops in the external ring are folded with a greater height than the remaining loops to form the apices to which the commissural points of the biological valve are attached.
- 30 6. A valve prosthesis according to claim 5, characterized in that each of the rings of the stent is made from a wire having a diameter of 0.55 mm and a loop height of approximately 8 mm and approximately 14 mm for the three greater loops, and that the cylindrical thread structure produced and the collapsible valve mounted thereon in a folded state have an outer diameter of approximately 10 mm and in

expanded state an outer diameter of approximately 30 mm.

7. A valve prosthesis according to claim 5, characterized in that three or more mutually attached rings placed on top of each other are used and that the stent is made to be fixed through the expansion at one point in the channel where the valve prosthesis is inserted, which point is different from the point where the valve is mounted in the stent.

10 8. A valve prosthesis according to any of the preceding claims, characterized in that the cylinder surface of the support means is closed to form a tubular element.

15 9. A balloon catheter for use in implantating a valve prosthesis according to any of the preceding claims and comprising a channel for injection of a fluid for the inflation of the balloon means of the catheter and an insertion cap wherein the balloon means of the catheter and a collapsible valve prosthesis mounted thereon are located during the injection, characterized in that the balloon means are provided with a profiled surface which is made to ensure a steady fastening of the valve prosthesis during the elimination of the balloon means from the protection cap and the subsequent inflation for expanding the stent.

25 10. A balloon catheter according to claim 9, characterized in that the profiling of the surface is made by beads or buds on the surface of the balloon means.

30 11. A balloon catheter according to claim 10, characterized in that the beads are placed in pairs in a number from four to eight along lines parallel with the longitudinal axis of the balloon means and with a spacing corresponding to the height of the stent used.

35 12. A balloon catheter according to claim 9, characterized in that the profiling of the surface is made by an indentation which is formed in the surface of the balloon means with an extension corresponding to the height of the stent used.

1/4

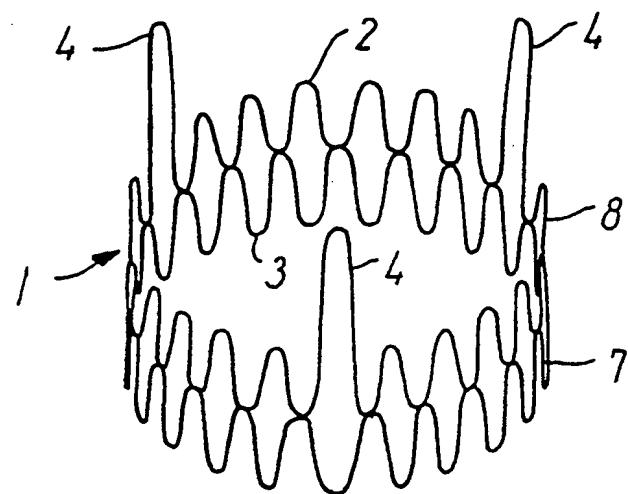


FIG. 1

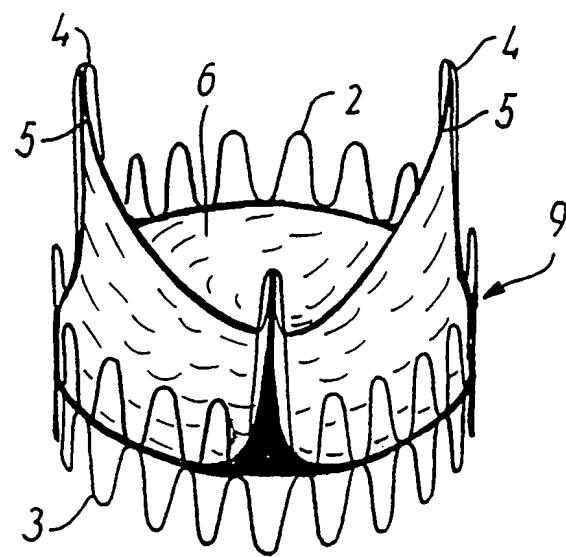


FIG. 2

2/4

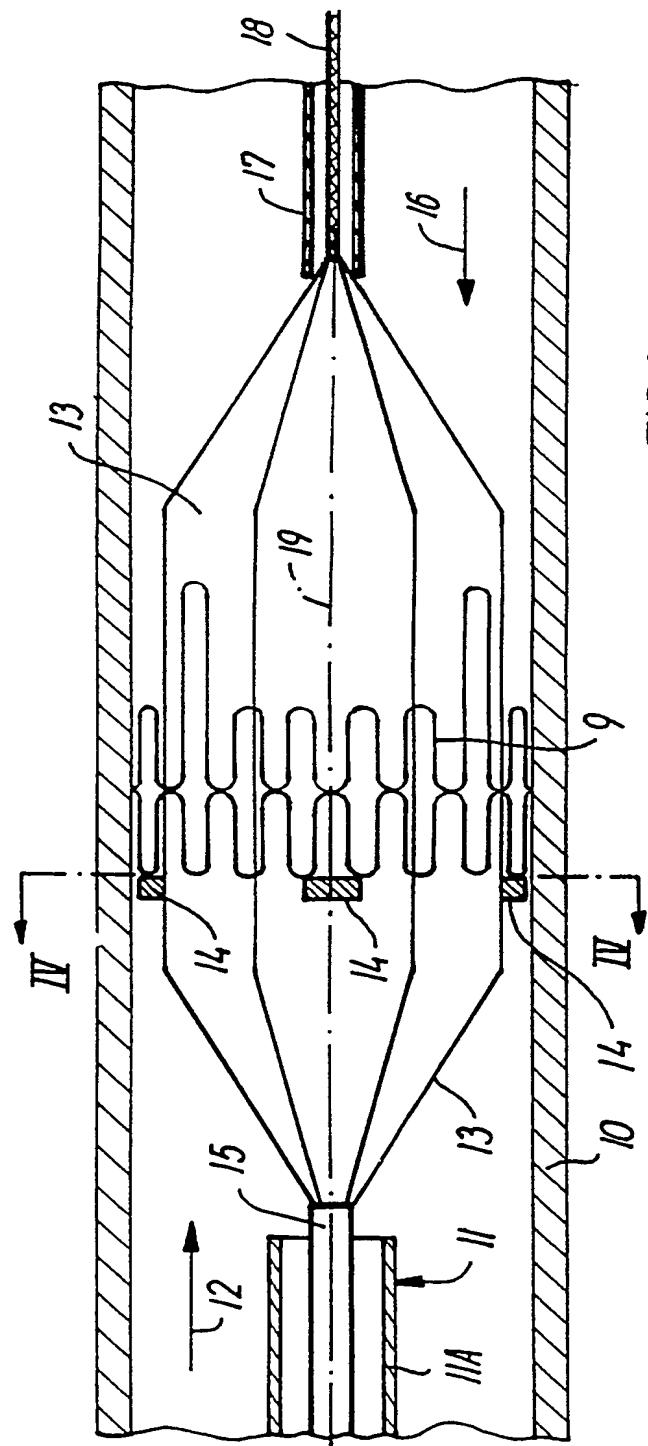


FIG. 3

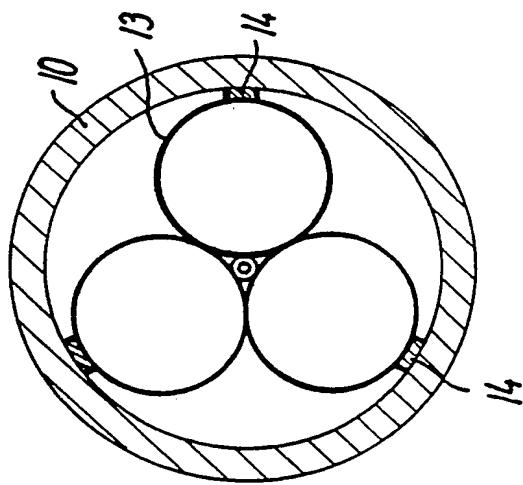


FIG. 4

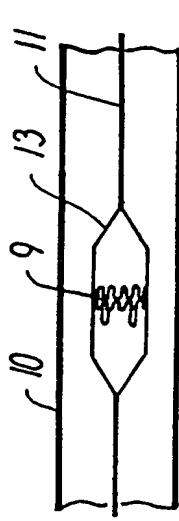


FIG. 5

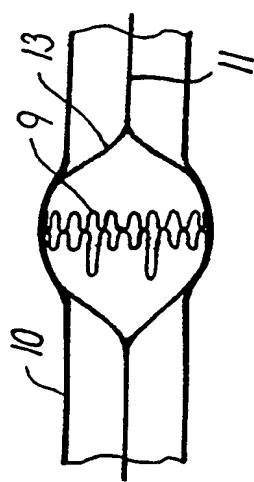


FIG. 6

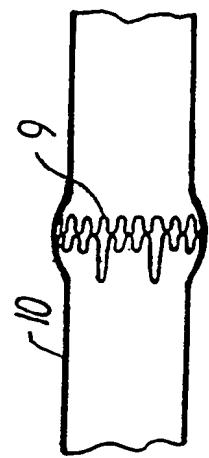


FIG. 7

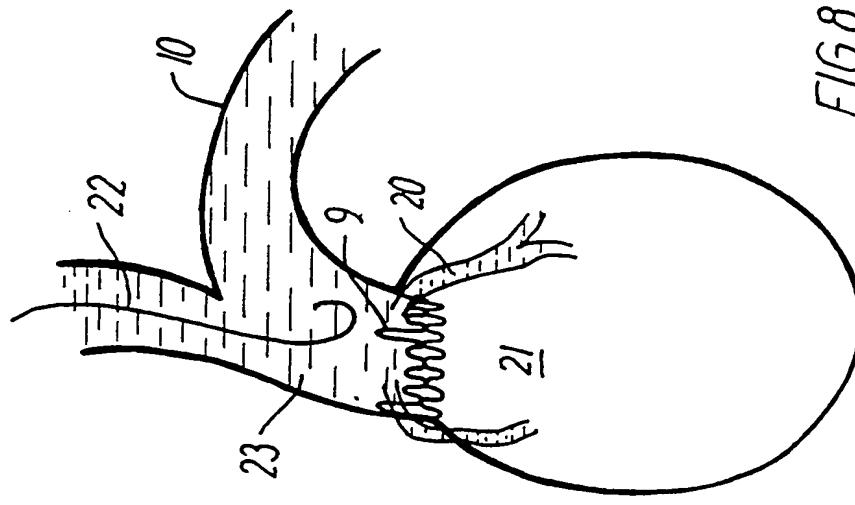


FIG. 8

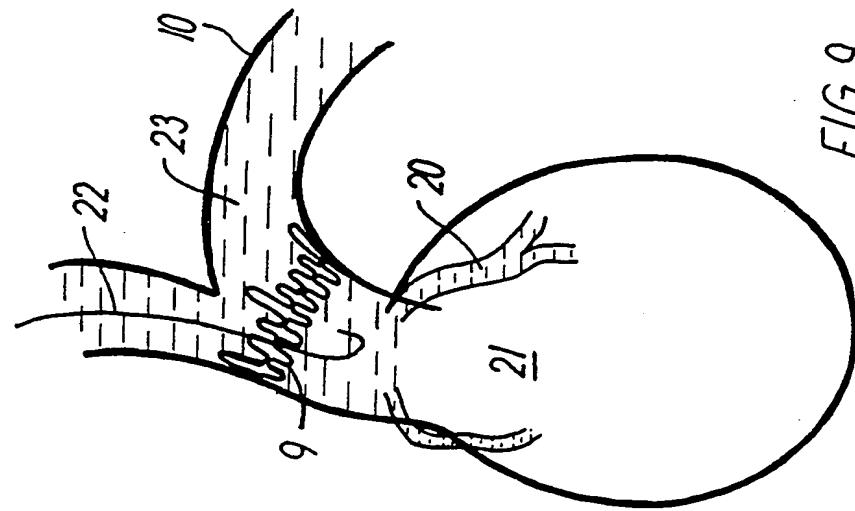


FIG. 9

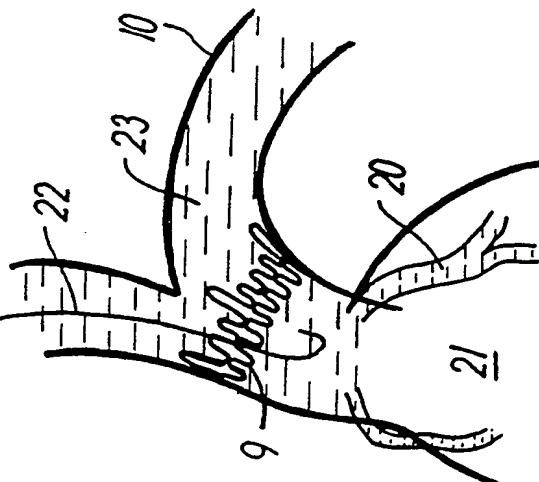
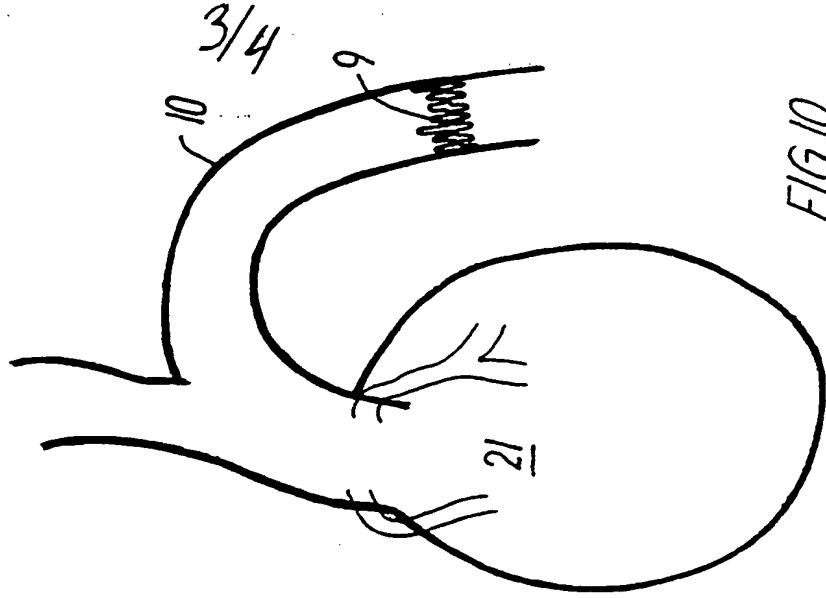
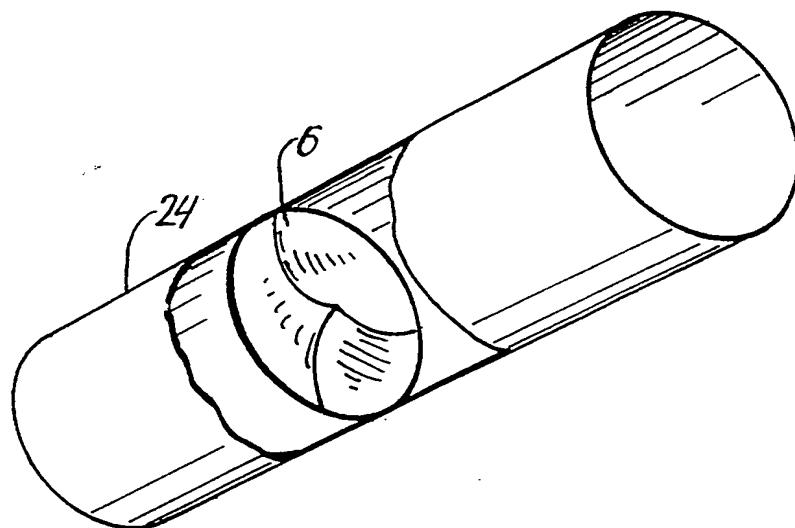
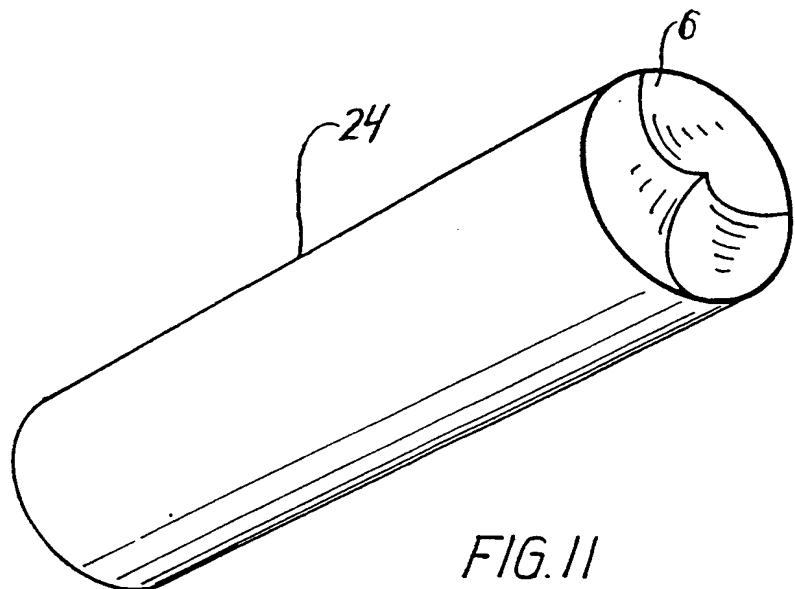


FIG. 10



4/4



INTERNATIONAL SEARCH REPORT

International Application No PCT/DK 91/00134

I. CLASSIFICATION OF SUBJECT MATTER (if several classification symbols apply, indicate all)⁶

According to International Patent Classification (IPC) or to both National Classification and IPC
IPC5: A 61 F 2/24, A 61 M 25/10

II. FIELDS SEARCHED

Minimum Documentation Searched⁷

Classification System	Classification Symbols
IPC5	A 61 B; A 61 F; A 61 M

Documentation Searched other than Minimum Documentation
 to the Extent that such Documents are Included in Fields Searched⁸

SE,DK,FI,NO classes as above

III. DOCUMENTS CONSIDERED TO BE RELEVANT⁹

Category ¹⁰	Citation of Document, ¹¹ with indication, where appropriate, of the relevant passages ¹²	Relevant to Claim No. ¹³
A	GB, A, 2056023 (DONALD NIXON ROSS) 11 March 1981, see figures 2,3 --	1-5,8
A	US, A, 3671979 (MOULOPoulos) 27 June 1972, see figures 2B,5 --	1,9
A	Derwent's abstract, No. 87-190 867/27, SU 1 271 508, publ. week 8727 (GORKII KIROV MEDICAL INS) -- -----	1

* Special categories of cited documents:¹⁰

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance, the claimed invention cannot be considered novel or cannot be considered to involve an inventive step

"Y" document of particular relevance, the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search

14th August 1991

Date of Mailing of this International Search Report

1991 -08- 21

International Searching Authority

Signature of Authorized Officer


 Leif Karnsäter

SWEDISH PATENT OFFICE

FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET

V. OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE¹

This international search report has not been established in respect of certain claims under Article 17(2) (a) for the following reasons:

1. Claim numbers....., because they relate to subject matter not required to be searched by this Authority, namely:

2. Claim numbers....., because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. Claim numbers....., because they are dependent claims and are not drafted in accordance with the second and third sentences of PCT Rule 6.4(a).

VI. OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING²

This International Searching Authority found multiple inventions in this international application as follows:

Claims 1-8 concerning a valve prosthesis.

Claims 9-12 concerning a catheter.

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims of the international application.

2. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims of the international application for which fees were paid, specifically claims:

3. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims. It is covered by claim numbers:

4. As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.

Remark on Protest

The additional search fees were accompanied by applicant's protest.
 No protest accompanied the payment of additional search fees.

ANNEX TO THE INTERNATIONAL SEARCH REPORT
ON INTERNATIONAL PATENT APPLICATION NO.PCT/DK 91/00134

This annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report.
The members are as contained in the Swedish Patent Office EDP file on **91-06-27**
The Swedish Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
GB-A- 2056023	81-03-11	US-A- 4343048	82-08-10
US-A- 3671979	72-06-27	NONE	

THIS PAGE BLANK (USPTO)